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## **CLAIMS**

- 1. Apparatus for producing attenuation corrected nuclear medicine images of patients, comprising:
- at least one gamma camera head that acquires nuclear image data suitable to produce a nuclear tomographic image at a first controllable rotation rate about an axis;
- at least one X-ray CT imager that acquires X-ray data suitable to produce an attenuation image for correction of the nuclear tomographic image at a second controllable rotation rate about the axis; and
- a controller that controls the data acquisition and first and second rotation rates to selectively provide at least one of the following modes of operation:
- (i) a movement gated NM imaging mode in which the second rotation rate is substantially higher than the first rotation rate and the data from each view of the X-ray acquisition is associated with one of a plurality of respiration gated time periods;
- (ii) a cardiac gated NM imaging mode in which the second rotation rate is substantially higher than the first rotation rate and the data from each view of the X-ray acquisition for different rotations is averaged, wherein the X-ray data is not correlated with the cardiac cycle; and
- (iii) a cardiac gated NM imaging mode in which the second rotation rate is higher than the first rotation rate and the X-ray data is binned in accordance with a same binning as the NM data.
- Apparatus according to claim 1 wherein the controller controls the data acquisition and first and second rotation rates to provide at least two of the modes of operation.
- Apparatus according to claim 1 wherein the controller controls the data acquisition and first and second rotation rates to provide all three of the modes of operation.
- A. Apparatus according to claim 1 or claim 2 wherein the provided modes of operation include at least mode (i).
- 5. Apparatus according to claim 1 or claim 2 wherein the provided modes of operation include at least mode (ii).

037/01051. A02

A nuclear medicine camera having an X-ray imaging capability, comprising: at least one gamma camera mounted on a gantry; and an X-ray CT imager mounted on the same gantry, wherein the at least one gamma camera and said X-ray imager are capable of simultaneously rotating about a common axis at different rotation rates.

8. A nuclear medicine camera according to claim 7 wherein the at least one gamma camera and said X-ray imager are capable of simultaneously rotating about a common axis at the same rotation rate.

A nuclear medicine camera having an X-ray imaging capability, comprising:

a gantry having a stationary portion and at least one rotating portion;

at least one gamma camera mounted on a said at least one rotating portion and capable

at least one gamma camera mounted on a said at least one rotating portion and capable of being rotated together at a common first rotation rate about an axis, said at least one gamma camera being capable of acquiring nuclear imaging data for reconstructing a tomographic nuclear image; and

an X-ray CT imager having an X-ray source mounted on said at least one rotating portion and being capable of acquiring X-ray imaging data for reconstructing an X-ray image;

said X-ray CT imager being mounted closer to said stationary portion than said at least one gamma camera.

10. A system according to claim 9 wherein the X-ray CT imager is mounted between the at least one gamma camera and stationary portion.

11. A system according to claim 9 wherein the at least one gamma camera comprises two gamma cameras.

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- 12. A system according to claim 11 wherein the two gamma cameras have a controllable angle between them and including a controller that controls the angle between the gamma cameras.
- 5 13. A system according to claim 10 wherein the at least one gamma camera comprises two gamma cameras.
  - 14. A system according to claim 13 wherein the two gamma cameras have a controllable angle between them and including a controller that controls the angle between the gamma cameras.
  - 15. A system according to any of claims 9-14 wherein the X-ray imager utilizes a fixed anode X-ray to produce X-rays.
- 15 16. A system according to any of claims 9-14 wherein the X-ray source is capable of simultaneously rotating about the axis at a rotation rate different from that of the rotation rate of the gamma camera.
- 17. A system according to claim 15 wherein the X-ray source is capable of simultaneously rotating about the axis at a rotation rate different from that of the rotation rate of the gamma camera.
  - 18. A method of mounting a CT imager on a gantry: determining a center of rotation of a rotor of the gantry;
- 25 siting a plurality of mounting elements at predetermined positions with respect to the center of rotation; and
  - attaching the mounting elements to the rotor while keeping the mounting elements at the predetermined positions.
- 30 19. A method according to claim 18 and including:

  providing a positioning jig referenced to said center of rotation; and
  attaching said mounting elements on said jig.

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- 20. A method according to claim 19 wherein said method comprises:
  centering a post at the center of rotation; and
  mounting said jig on said post.
- 5 21. A method according to any of claims 18-20 and including:

  providing an X-ray source wherein the source is referenced to a first mounting reference thereon;

providing an X-ray detector system wherein the detector is referenced to a second mounting surface thereon; and

- mounting the X-ray source and X-ray detector on said attached mounting elements.
- 22. A method according to claim 21 wherein the mounting elements comprise alignment elements which mate with matching elements on the first and second mounting references.
- 15 23. A method according to any of claims 18-20 wherein attaching comprises gluing.
  - 24. A method according to any of claims 18-20 wherein attaching comprises attaching with screws.
- 20 25. A method according to claim 21 wherein attaching comprises gluing.
  - 26. A method according to claim 21 wherein attaching comprises attaching with screws.
  - 27. A method according to claim 22 wherein attaching comprises gluing.
  - 28 A method according to claim 22 wherein attaching comprises attaching with screws.
  - 29. A method of nuclear imaging, including acquiring attenuation data for correcting the nuclear image, comprising:
- acquiring nuclear emission data over a first axially extending portion of the body;

  determining an extent of a radioactive region of interest in the body; and

  acquiring transmission data over a second axially extending portion of the body,

  responsive to the determined extent.

037/01051, A02

30. A method according to claim 29 wherein the second axially extending portion is smaller than the first axially extending portion.

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- 31. A method according to claim 29 or claim 30 wherein determining an extent comprises acquiring a planar nuclear emission image.
- 32. A method according to claim 29 or claim 30 wherein determining an extent comprises: determining said extent from said acquired nuclear emission data.

33. A method according to claim 29 or claim 30 wherein the transmission data is acquired using an X-ray source.

34. A method according to claim 29 or claim 30 wherein the transmission data is acquired using a gamma ray source.

- 35. A method according to claim 31 wherein the transmission data is acquired using an X-ray source.
- 20 36. A method according to claim 31 wherein the transmission data is acquired using a gamma ray source.
  - 37. A method according to claim 32 wherein the transmission data is acquired using an X-ray source.
  - 38. A method according to claim 32 wherein the transmission data is acquired using a gamma ray source.
- 39. A method according to claim 33 wherein the transmission data is acquired using an X-30 ray source.
  - 40. A method according to claim 33 wherein the transmission data is acquired using a gamma ray source.

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- A method of acquiring attenuation data for correcting a nuclear image, comprising: 41. determining an extent of an organ of interest in the body;
- acquiring nuclear emission data over a first axially extending portion of the body larger than the organ of interest; and

acquiring transmission data over a second axially extending portion of the body, responsive to the determined extent of the organ, said second portion being substantially smaller than the first portion.

- A method according to claim 41 wherein determining an extent comprises acquiring a 42. 10 planar X-ray image.
  - A method according to claim 41 or claim 42 wherein the transmission data is acquired
  - A method according to claim 41 wherein determining an extent comprises acquiring a 44. planar transmission gamma ray image.
  - A method according to claim 41 or claim 44 wherein the transmission data is acquired 45. using a gamma ray source
  - A method according to claim 41 wherein determining an extent comprises acquiring a 46. planar nuclear emission image.
- A method according to claim 41 wherein determining an extent comprises: 25 47. determining said extent from said acquired nuclear emission data.
- A method of producing a nuclear medicine image of a subject, comprising: 48. acquiring nuclear imaging data suitable to produce a nuclear tomographic image, said nuclear image data being acquired by a gamma camera head rotating about the subject; 30

acquiring X-ray imaging data suitable to produce an X-ray tomographic image for attenuation correction of the gamma camera image, said X-ray imaging data being acquired by detectors irradiated by an X-ray source rotating around the subject;

reducing the sensitivity of gamma camera head while the X-rays are produced; and reconstructing an attenuation corrected nuclear medicine image utilizing the nuclear imaging data and X-ray imaging data.

- A method according to claim 48 wherein the gamma camera head includes a plurality of 5 49. photomultiplier tubes having dynodes, wherein reducing the sensitivity includes reducing voltages on said dynodes.
  - A method of producing a nuclear medicine image of a subject, comprising **30.** acquiring nuclear imaging data suitable to produce a nuclear tomographic image, said nuclear image data being acquired by a gamma camera head rotating about the subject;

acquiring X-ray imaging data suitable to produce an X-ray tomographic image for attenuation correction of the gamma camera image, said X-ray imaging data being acquired by detectors irradiated by an X-ray source rotating around the subject for a plurality of rotations;

averaging X-ray imaging data of a same view taken at different rotations of the X-ray source to produce averaged X-ray imaging data;

reconstructing an attenuation corrected gated nuclear medicine image utilizing the nuclear imaging data and averaged ungated X-ray imaging data.

- Apparatus for producing attenuation corrected nuclear medicine images of patients, 51. comprising;
- a plurality of gamma camera heads that acquire nuclear image data suitable to produce a nuclear tomographic image at a plurality of positions about an axis;
- at least one X-ray CT imager that acquires X-ray data suitable to produce an attenuation image for correction of the nuclear tomographic image at a plurality of positions about and axis, said X-ray CT imager comprising a stationary anode X-ray tube.
- Apparatus for producing a nuclear medicine image of a subject, comprising: 52.
- at least one gamma camera having at least one detector mounted on a gantry and capable of rotating about an axis and of acquiring nuclear imaging data suitable to produce a nuclear tomographic image;
- a C-T X-ray imager including an X-ray source, mounted on said gantry and capable of rotating about the axis and X-ray detectors separate from detectors of the gamma camera,

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037/01051 A02

acquiring X-ray imaging data suitable to produce an X-ray tomographic image for attenuation correction of the gamma camera image; and

circuitry capable of reconstructing an attenuation corrected nuclear medicine image utilizing the nuclear imaging data and X-ray imaging data, said C-T X-ray imager having a capability of producing a C-T image having an RMS noise level of only about 10 Hounsfield numbers or more.

- 53. Apparatus according to claim 52 wherein the RMS noise level is more than 15 Houndsfield numbers.
- 54. Apparatus according to claim 52 wherein the RMS noise level is more than 20 Houndsfield numbers.
- 55. Apparatus according to claim 52 wherein the RMS noise level is more than 50 Houndsfield numbers.
- 56. Apparatus according to claim 52 wherein the RMS noise level is more than 100 Houndsfield numbers.
- 20 57. Apparatus according to claim 52 wherein the RMS noise level is less than about 200 Houndsfield numbers.
  - 58. Apparatus according to any of claims 52-57 the X-ray imager is only capable of producing a tomographic image having a resolution poorer than about 2 lp/cm in a transaxial direction.
  - 59. Apparatus according to claim 58 wherein the resolution is poorer than about 3 lp/cm.
  - 60. A apparatus according to claim 58 wherein the resolution is poorer than about 4 lp/cm.
  - 61. Apparatus for producing a nuclear medicine image of a subject, comprising:

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037/01051 A02

## PCT://2 99/00300 PEAUS 21 AUG 2001

at least one gamma camera having at least one detector mounted on a gantry and capable of rotating about an axis and of acquiring nuclear imaging data suitable to produce a nuclear tomographic image;

a C-T X-ray imager including an X-ray source, mounted on said gantry and capable of rotating about the axis and X-ray detectors separate from detectors of the gamma camera, acquiring X-ray imaging data suitable to produce an X-ray tomographic image for attenuation correction of the gamma camera image; and

circuitry capable of reconstructing an attenuation corrected nuclear medicine image utilizing the nuclear imaging data and X-ray imaging data, said C-T X-ray imager having a capability of producing a C-T image having a resolution of only about 2 lp/cm or less.

- Apparatus according to claim 61 wherein the resolution is poorer than about 3 lp/cm. 62.
- Apparatus according to claim 61 wherein the resolution is poorer than about 4 lp/cm. 63.